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Three-dimensional kinematic correlates of ball velocity during maximal instep football kicking.

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Three-dimensional kinematic correlates of ball velocity during maximal instep soccer

kicking in males.

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Abstract

Achieving a high ball velocity is important during soccer shooting, as it gives the goalkeeper less time to react, thus improving a player's chance of scoring and is also fundamental to long passes and goalkicks. This study aimed to identify important technical aspects of kicking linked to the generation of ball velocity using regression analyses. Maximal in-step kicks were obtained from twenty-two academy level soccer players using a ten camera motion capture system sampling at 500 Hz. Three-dimensional kinematics of the lower extremity segments were obtained. Regression analysis was used to identify the kinematic parameters associated with the development of ball velocity. A single biomechanical parameter; knee extension velocity of the kicking limb at ball contact Adj $R^2=0.37$, $p \leq 0.01$ was obtained as a significant predictor of ball-velocity. This study suggests that sagittal plane knee extension velocity is the strongest contributor to ball velocity and potentially overall kicking performance. It is conceivable therefore, that players may benefit from exposure to coaching and strength techniques geared towards the improvement of knee extensors strength as highlighted in this study.

Introduction

Kicking is a fundamental motor skill in soccer (Lees & Nolan, 1998) and the in-step soccer kick is the most frequently analysed action in soccer (Zernicke & Roberts, 1976; Asami & Nolte, 1983; Putnam & Dunn, 1987; Dorge et al., 1999; Kellis & Katis, 2007; Lees et al., 2010; De Witt & Hinrichs, 2012). It is important to achieve a high ball velocity in soccer goal kicking, since first and foremost this gives the goalkeeper less time to react thus improving a player's chance of scoring but is also fundamental to long passes and goalkicks (Dorge, Anderson, Sorensen, & Simonsen, 2002).

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3 51 The velocity of the ball subsequent to the kicking action is therefore considered a central
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5 52 biomechanical indicator of kicking performance and it is the consequence of several factors
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7 53 such as kicking technique/ kinematics (Lees & Nolan, 1998), approach velocity/ angulation
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9 54 (Isokawa & Lees, 1988; Kellis, Katis & Gissis, 2004), skill level (Commetti, Maffiuletti,
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11 55 Pousson, Chatard, & Maffulli, 2001; Luhtanen, 1988), kicking limb (Barfield, 1995; Dorge et
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13 56 al., 2002; Narici, Sirtori, & Mognoni, 1988; Nunome, Ikegami, Kozakai, Apriantono, &
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15 57 Sano, 2006), and age (Lees & Nolan, 1998). However, although previous analyses have
16
17 58 attempted to relate the resultant ball velocity to several determining factors, the majority have
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19 59 been comparative in nature in that they have aimed to identify similarities and differences
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21 60 between in-step kicking conditions. Therefore, despite the wealth of research into the
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23 61 mechanics of in-step kicking, the specific factors associated with the generation of ball
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25 62 velocity are not yet fully established.
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34 64 During in-step kicking the lower extremity segments interact via a proximal to distal
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36 65 mechanism along the kinematic chain in order to transfer momentum to the kicking foot
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38 66 (Putnam, 1993; De Witt & Hinrichs 2012). Thus far De Witt & Hinrichs (2012) have
39
40 67 performed the only investigation using correlational analyses in an attempt to determine the
41
42 68 mechanical factors associated with the development of ball velocity. Velocity of the foot
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44 69 centre of mass, velocity of the foot centre of mass relative to the knee and peak velocity of
45
46 70 the knee relative to the hip at ball impact were shown to be significantly correlated with ball
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48 71 velocity. However De Witt & Hinrichs (2012) were more concerned with the mechanical
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50 72 determinants of ball velocity and thus examined few kinematic parameters that were limited
51
52 73 primarily to the sagittal plane. Furthermore, this investigation utilized single correlational
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54 74 analyses rather than multiple regression; thus the weighted influence of the discrete kinematic
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56 75 parameters on ball velocity was not determined.
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77 Whilst the importance of maximal instep kicking has been well documented in terms of its
78 influence on performance, there has been little attention paid to the kinematic elements
79 pertinent to the development of ball velocity. This study therefore aimed to identify important
80 lower extremity rotational aspects of in-step kicking pertinent to the generation of high ball
81 velocity using three dimensional (3-D) kinematic modelling and regression analyses.

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83

84 **Methods**

85 *Participants*

86 Twenty-two male soccer players (age = 16.8 ± 0.71 years; height = 1.80 ± 0.07 m; mass =
87 76.73 ± 8.31 kg) were examined whilst kicking a stationary soccer ball (size 5) as hard as
88 possible into a regulation sized goal using their right (dominant) foot. Participants were
89 academy level players contracted to a top-division professional soccer club in England.
90 Participants were all free from musculoskeletal pathology at the time of data collection and
91 provided written informed consent in accordance with the predetermined guidelines outlined
92 in the declaration of Helsinki. Ethical approval was provided by a University ethical board.

93

94 *Procedures*

95 A ten camera motion analysis system (Qualisys™ Medical AB, Gothenburg, Sweden)
96 captured 3-D kinematic data from the lower extremities at 500 Hz from each participant
97 performing maximal instep kicks with a 5m run up and an approach angle of 45° in
98 accordance with Isokawa & Lees (1988). The ball was positioned such that it allowed the
99 support foot to land on a piezoelectric force platform (Kistler Instruments, Model 9281CA)
100 which sampled at 1000 Hz. In accordance with the protocol outlined by Shan & Westerhoff

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3 101 (2005) the camera system also tracked the soccer ball using three reflective markers, thus
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5 102 allowing ball release speed to be quantified. Dynamic calibration of the motion analysis
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7 103 system was performed before each data collection session using predefined acceptance
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9 104 criteria with an identical motion capture system (Sinclair et al., 2013).
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11 105
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13 106 The calibrated anatomical systems technique (CAST) marker configuration was utilized for
14
15 107 this study (Cappozzo, Catani, Leardini, Benedetti, & Della, 1995). Retro reflective markers
16
17 108 were positioned on the following anatomical locations; bilaterally to the 1st and 5th
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19 109 metatarsal heads, calcaneus, medial and lateral malleoli, medial and lateral epicondyle of the
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21 110 femur, greater trochanter, posterior superior iliac spine (PSIS) and right and left anterior superior
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23 111 iliac spine (ASIS). Tracking clusters were positioned on the right and left thigh and right and
24
25 112 left shank. The tracking clusters were comprised of four 19mm spherical reflective markers
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27 113 mounted to a thin sheath of lightweight carbon fiber with a length to width ratios of 1.5:1 and
28
29 114 2.05:1, in accordance with the previously established guidelines (Cappozzo, Cappello, Della-
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31 115 Croche & Pensalfini, 1997). This allowed the pelvis, bilateral foot, shank and thigh segments
32
33 116 to be defined and tracked. The proximal joint centre for the thigh segment was quantified
34
35 117 using regression equations via the positions of the ASIS markers (Bell, Brand, & Pedersen,
36
37 118 1989). A static trial was captured to define the pelvis, thighs, feet and shank segments of both
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39 119 the left and right limbs, following which markers used only to define the segments, were
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41 120 removed prior to the collection of dynamic information.
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49 122 *Data Processing*

50
51 123 3-D Kinematic measures were calculated using Visual 3-D (C-Motion Inc, Germantown,
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53 124 USA) and filtered at 100 Hz using a zero-lag low-pass Butterworth 4th order filter. Ten trials
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55 125 of maximal instep kicking were averaged for each participant. Trials were defined by the
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3 126 instances of stance limb footstrike with a force platform (Sinclair et al., 2011) to ball contact.
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5 127 Ball contact was determined using retro-reflective marker tape attached to the ball (Shan &
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7 128 Westerhoff, 2005). Angular kinematics from the hip, knee and ankle joints were created
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9 129 about an XYZ cardan sequence referenced to co-ordinate systems created about the proximal
10
11 130 end of the segment, where X = sagittal plane rotations; Y = coronal plane rotations and Z =
12
13 131 transverse plane rotations (Lees et al., 2010). Three-dimensional kinematic measures of both
14
15 132 stance and kicking limbs from the hip, knee and ankle which were extracted for statistical
16
17 133 analysis were 1) angle at footstrike, 2) angle at ball impact, 3) range of motion during stance,
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19 134 4) peak angle during stance, 5) relative range of motion from footstrike to peak angle, 6)
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21 135 angular velocity at footstrike, 7) angular velocity at ball impact and 8) peak angular velocity.
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27 137 *Statistical analyses*

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29 138 A factor analysis was used to select a smaller number of variables to be included in the
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31 139 regression analysis. This preliminary analysis yielded 10 separate factors, and the variables
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33 140 with the highest loading for each factor were extracted. These factors were then entered into
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35 141 the multiple regression analyses which was conducted with ball velocity as criterion and the
36
37 142 3-D kinematic parameters as independent variables. The significance level for the regression
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39 143 model was set at the $p \leq 0.05$ level. The independent variables were examined for co-linearity
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41 144 prior to entry into the regression model using a Pearson's correlation coefficient matrix and
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43 145 those exhibiting high co-linearity $R \geq 0.7$ were removed. All statistical procedures were
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45 146 conducted using SPSS 20.0 (SPSS Inc, Chicago, USA).
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51 148 **Results**

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53 149 *Ball velocities and Regression analyses*
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3 150 Tables 1-2 present the mean \pm standard deviation 3-D kinematic parameters from both the
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5 151 stance and kicking limbs. The results revealed mean \pm standard deviation ball velocities of
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7 152 $26.73 \pm 6.47 \text{ m}\cdot\text{s}^{-1}$. The overall regression model was significant and yielded an Adj R^2 of
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9
10 153 $0.37, p \leq 0.01$. A single biomechanical parameter, peak knee extension velocity of the kicking
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12 154 limb in the sagittal plane was obtained as a significant predictor of ball velocity ($B=0.55$,
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14 155 $t=3.86$) Adj $R^2=0.37, p \leq 0.01$.

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158 @@@ Table 1 near here @@@

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160 @@@ Table 2 near here @@@

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162 **Discussion**

163 The aim of the current investigation was to determine the lower extremity 3-D kinematic
164 parameters pertinent to the development of ball velocity during maximal in-step kicking. This
165 study represents the first to examine these factors during maximal in-step kicking in soccer.

166

167 The regression analysis revealed that knee extension angular velocity of the kicking limb at
168 ball impact was the only significant predictor of ball velocity. The fit of the multiple
169 regression analysis ($R^2 = 0.37$) suggests that variance in ball velocity may be significantly
170 influenced by the kicking technique employed by the player. This concurs with the Lees &
171 Nolan (1996) proposition that variations in ball velocity during in-step kicking are influenced
172 by alterations in kicking kinematics.

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3 174 That knee extension angular velocity at ball contact served as a significant predictor of ball
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5 175 velocity is unsurprising and is in line with the observations of Ball (2008) who found that
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7 176 peak knee angular velocity was significantly related to ball velocity during Australian Rules
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9 177 soccer punt kicking. This finding reinforces the notion that the velocity of the foot centre of
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11 178 mass which ultimately governs the resultant ball velocity is a function of the angular velocity
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13 179 of the shank in the sagittal plane (Ball, 2008). The linear velocity of the rotating foot which
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15 180 makes contact with the ball is proportional to the product of the angular velocity and radius
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17 181 rotation of the proximal body segments (Ball, 2008) thus the significant relationship between
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19 182 shank angular velocity and ball velocity appears logical.
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25 184 The findings of this study may allow recommendations for specific training modifications to
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27 185 be made with the goal order of improving ball velocity during in-step soccer kicking. It has
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29 186 been recognized that performing training drills that promote greater foot velocities and shank
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31 187 angular velocities, are useful methods of training this skill (Ball, 2007). Therefore to improve
32
33 188 ball velocity it is recommended that coaching practices be implemented with the purpose of
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35 189 increasing sagittal plane knee angular velocity. There is further indication an effective
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37 190 strength training program which encompasses both concentric and eccentric training
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39 191 modalities also improves kicking distance and power (DeProft, Cabri, Dufour, & Clarys,
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41 192 1988). Cabri, De Proft, Dufour, & Clarys (1988) detected significant correlations between
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43 193 knee flexor and extensor strength and kick distance. Correspondingly Poulmedis (1988) and
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45 194 Narici et al. (1988) also found strong correlations between lower extremity muscle strength
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47 195 and resultant ball velocity. Therefore as the principal contributor to knee extension, the
48
49 196 quadriceps muscle group generates high intensity forces during the in-step kick (Lees,
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51 197 Bartona, & Robinson, 2010). Hence, from a biomechanical perspective, strength training of
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53 198 the quadriceps muscle group may be of particular importance to soccer players wishing to
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3 199 improve their scoring potential through increases in ball velocity. It is also recommended
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5 200 based on this observation that the hamstrings also receive strength training as not to
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7 201 negatively influence the quadriceps: hamstrings strength ratio which has been linked to the
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9 202 development of injury when it falls outside the recommended 3:2 ratio (Coombs & Garbutt,
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11 203 2002).

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16 205 Although statistically significant the regression model suggests that there remains variance in
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18 206 ball velocity that was not accounted for by the discrete kinematic measures that were entered
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20 207 into the multiple regression analysis. Some of the remaining variance may be attributable to
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22 208 the collision mechanics between foot and ball which have been reported by various authors as
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24 209 pertinent to kicking tasks (Nunome et al., 2006). Bull-Andersen, Dorge, & Thomsen (1999)
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26 210 noted that ball velocity during soccer in-step kicking was a product of foot velocity and the
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28 211 coefficient of restitution between foot and ball. Lastly, whilst this investigation examined the
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30 212 influence of the lower extremities kinematics on resultant ball velocity, no information was
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32 213 examined regarding the influence of upper body kinematics on the resultant ball velocity.
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34 214 Chen & Chang (2010) showed that arm swing can significantly influence the resultant ball
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36 215 velocity. Similarly Shan & Westerhoff (2005) showed that effective upper-body movement to
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38 216 be a key factor in creating better initial conditions for a more explosive muscle contraction
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40 217 during kicking. It permits a more powerful quasi whip-like movement of the kicking leg. As
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42 218 such it is recommended that future examinations be conducted to investigate the upper body
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44 219 contribution to ball velocity during in-step kicking.
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52 221 A limitation of the present study was the all-male sample may limit its generalizability as
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54 222 Barfield, Kirkendall, & Yu (2002) documented kinematic differences in kicking kinematics
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56 223 during the maximal instep soccer kick. There remains currently a noticeable paucity of
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3 224 research regarding the mechanics of in-step kicking in females, and the growth in female
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5 225 participation in soccer has failed to lead to a corresponding growth in the study of the
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7 226 mechanics of kicking in females. It is therefore recommended that the current investigation
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9 227 be repeated using a female sample.
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14 229 In addition, although ball velocity has been the focus of a number of examinations in soccer,
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16 230 there is currently a lack of published studies examining the discrete 3-D kinematic parameters
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18 231 associated with accuracy during in-step kicking. It was proposed by Godik, Fales, & Blashak
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20 232 (1993) that kicks with the greatest ball velocity are also associated with the highest degree of
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22 233 accuracy, and conversely Teixeira (1999) showed that that higher ball velocities were linked
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24 234 to reductions in accuracy. Lees & Nolan, (1998) comparing the mechanics of in-step kicking
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26 235 with a focus on both accuracy and ball velocity, found that when accuracy is paramount there
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28 236 is a decrease in lower extremity joint angular velocities and ball velocity compared to
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30 237 maximal velocity kicking. This leads to the notion that a trade-off exists between accuracy
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32 238 and ball velocity. Whilst ball velocity has been linked to performance, the accuracy of in-step
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34 239 kicking is also clearly pertinent as the kick still has to hit a specific target in order for a goal
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36 240 to be scored. Given the lack of published work investigating the mechanics of accurate
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38 241 kicking it is recommended therefore that future analyses consider the discrete kinematic
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40 242 factors associated with the development of accuracy during in-step soccer kicking.
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48 244 In conclusion this study provides new information regarding the 3-D kinematic parameters
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50 245 associated with the development of ball velocity during in-step kicking. The current
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52 246 investigation documents that knee extension angular velocity is most pertinent to the
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54 247 development of ball velocity during in-step kicking. It is recommended that training
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3 248 modalities be modified towards increasing this measure for those wishing to improve their
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5 249 kicking performance.

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3 347 Table 1: Hip, knee and ankle joint angular parameters (means \pm SD) from the kicking and
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5 348 stance limbs limb.
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8 349 Table 2: Hip, knee and ankle joint angular velocities (means \pm SD from the kicking and stance
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10 350 limbs limb.
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For Peer Review Only

	Hip		Knee		Ankle	
Sagittal Plane (+ =flexion/ - =extension)	Kick	Stance	Kick	Stance	Kick	Stance
Angle at Footstrike (°)	-16.56 + 12.93	54.52 + 12.27	77.26 + 15.52	26.01 + 7.02	44.78 + 14.06	83.64 + 10.29
Angle Ball impact (°)	12.97 + 14.27	13.10 + 10.84	42.03 + 13.48	40.56 + 9.61	53.55 + 22.42	78.89 + 12.51
Range of Motion (°)	29.79 + 6.19	41.42 + 7.10	35.23 + 10.61	14.55 + 5.52	8.78 + 4.17	4.75 + 3.77
Peak Range of Motion (°)	29.78 + 9.19	0.13 + 1.12	23.22 + 7.16	19.04 + 5.03	10.75 + 5.06	17.55 + 10.76
Peak Angle (°)	13.49 + 8.57	54.52 + 21.70	100.48 + 13.80	45.04 + 17.57	55.26 + 21.51	65.89 + 24.41
Coronal plane (+ =adduction/ - =abduction)						
Angle at Footstrike (°)	-10.69 + 4.91	-7.73 + 6.99	-6.17 + 13.61	6.59 + 7.14	-5.14 + 10.41	0.42 + 8.75
Angle Ball impact (°)	-15.55 + 4.74	11.28 + 7.95	-6.02 + 9.45	5.20 + 10.44	-11.38 + 13.15	-9.59 + 8.68
Range of Motion (°)	4.86 + 5.01	18.51 + 3.62	0.15 + 1.60	1.38 + 3.17	6.25 + 5.31	10.02 + 6.17
Peak Range of Motion (°)	9.05 + 6.60	18.51 + 4.11	-8.16 + 11.34	3.65 + 4.77	6.24 + 5.48	13.61 + 4.78
Peak Angle (°)	-19.74 + 4.96	11.27 + 8.54	1.99 + 3.89	2.94 + 8.50	-11.38 + 13.14	-13.61 + 4.78
Transverse plane (+ =internal/ - =external)						
Angle at Footstrike (°)	-6.78 + 16.18	-4.04 + 15.95	-3.53 + 6.14	-20.17 + 14.61	-12.15 + 7.78	-20.17 + 14.61
Angle Ball impact (°)	-1.70 + 15.95	-10.13 + 16.54	-9.04 + 9.22	-8.56 + 11.89	-9.58 + 10.46	-8.56 + 11.89
Range of Motion (°)	5.09 + 6.19	6.09 + 7.70	5.20 + 3.17	11.60 + 9.18	2.58 + 3.69	11.61 + 8.89
Peak Range of Motion (°)	11.70 + 7.11	9.69 + 6.68	5.98 + 2.97	14.96 + 8.97	4.28 + 5.01	14.96 + 7.98
Peak Angle (°)	4.92 + 15.88	-13.74 + 16.43	-9.52 + 6.51	-5.21 + 10.55	-7.87 + 8.01	-5.21 + 10.55

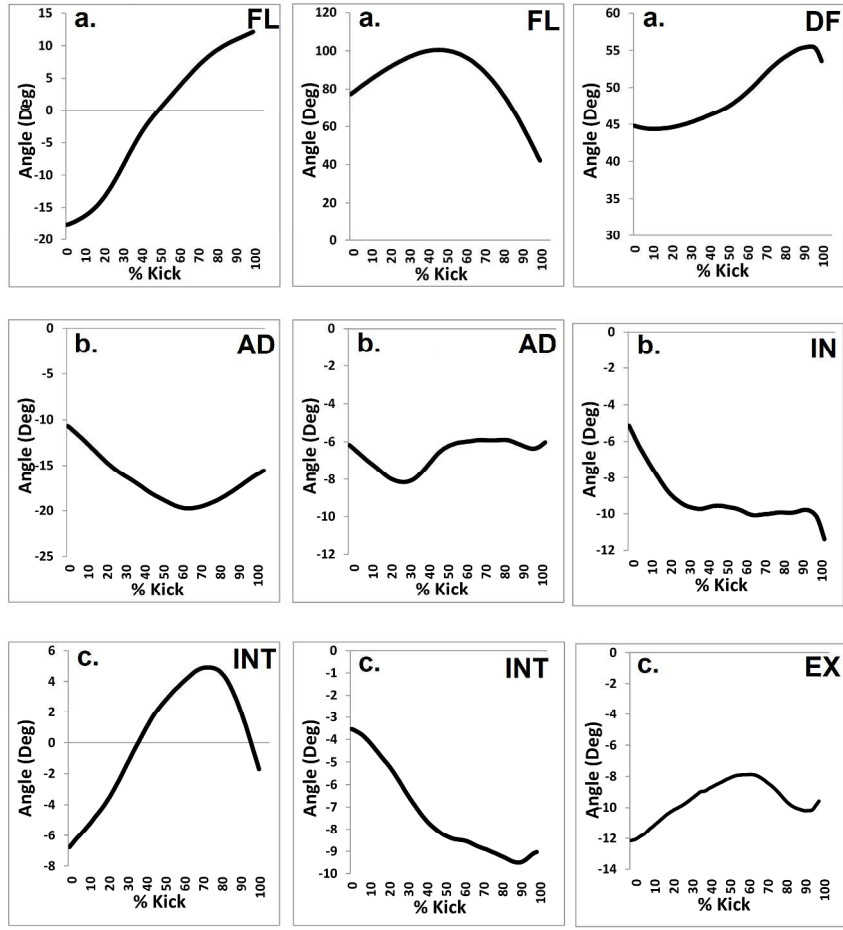
	Hip		Knee		Ankle	
Sagittal Plane (+ =flexion/ - =extension)	Kick	Stance	Kick	Stance	Kick	Stance
Velocity at Footstrike ($^{\circ} \cdot s^{-1}$)	40.32 + 130.38	-302.91 + 148.47	575.32 + 168.96	-38.31 + 168.56	-59.16 + 191.12	-375.81 + 187.42
Velocity at Ball impact ($^{\circ} \cdot s^{-1}$)	161.93 + 201.04	-255.52 + 178.14	-1563.13 + 579.19	-157.98 + 133.35	-627.64 + 445.07	-36.32 + 116.18
Peak Velocity ($^{\circ} \cdot s^{-1}$)	367.15 + 160.68	-595.42 + 342.91	-1563.13 + 579.19	751.36 + 424.55	169.98 + 262.88	-750.40 + 508.18
Coronal plane (+ =adduction/ - =abduction)						
Velocity at Footstrike ($^{\circ} \cdot s^{-1}$)	-73.00 + 99.26	166.12 + 154.74	-41.25 + 147.25	-23.34 + 94.94	-139.20 + 187.92	-119.68 + 202.63
Velocity at Ball impact ($^{\circ} \cdot s^{-1}$)	174.98 + 166.15	78.84 + 99.63	92.67 + 353.16	-23.88 + 81.40	-201.51 + 273.98	70.92 + 90.35
Peak Velocity ($^{\circ} \cdot s^{-1}$)	-113.97 + 119.83	300.32 + 265.11	-110.04 + 195.82	157.05 + 245.18	38.33 + 145.34	657.21 + 704.27
Transverse plane (+ =internal/ - =external)						
Velocity at Footstrike ($^{\circ} \cdot s^{-1}$)	156.67 + 148.10	-27.60 + 111.65	43.52 + 119.31	191.33 + 227.09	-130.41 + 190.88	2.87 + 151.67
Velocity at Ball impact ($^{\circ} \cdot s^{-1}$)	-222.57 + 285.59	75.94 + 140.26	5.23 + 345.90	-75.67 + 165.32	-244.97 + 441.74	46.48 + 141.09
Peak Velocity ($^{\circ} \cdot s^{-1}$)	190.88 + 120.09	175.39 + 206.66	-86.03 + 214.60	342.12 + 386.52	49.86 + 159.13	-315.81 + 344.54

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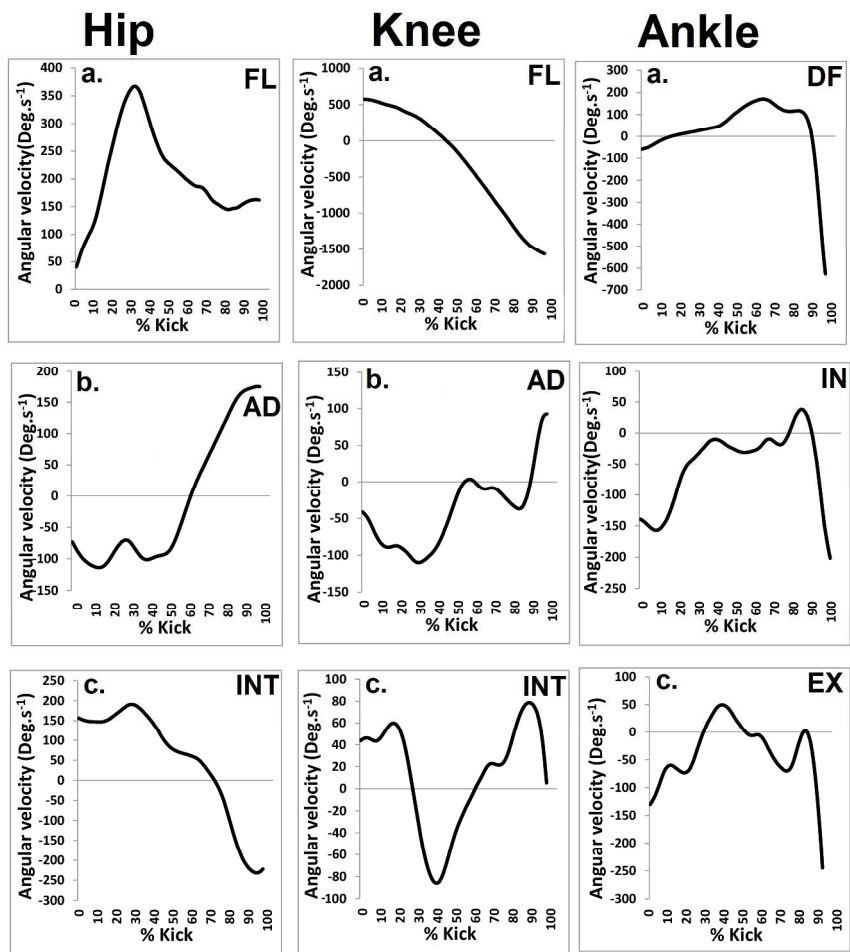
Hip

Knee

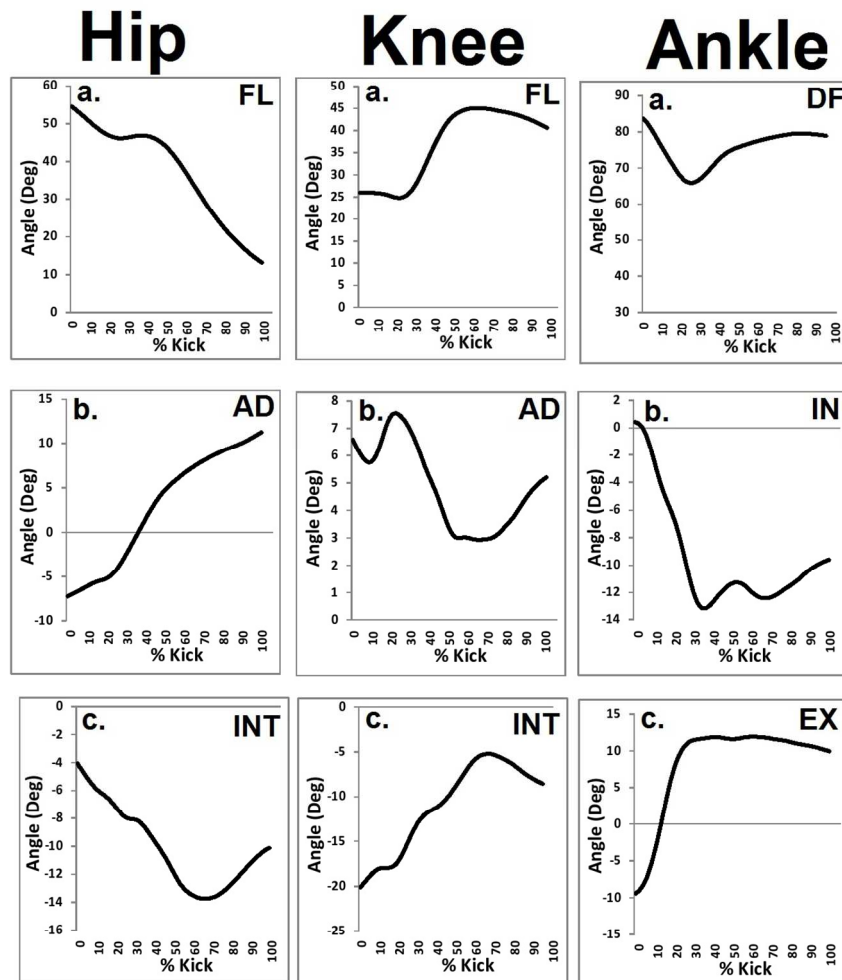
Ankle



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