Bioprosthetic valve thrombosis and degeneration following transcatheter aortic valve implantation (TAVI).

Abstract:

Bioprosthetic valve thrombosis (BPVT) is a recognised complication of prosthetic aortic valves and can be seen in up to 13% of patients after transcatheter implantation. The mechanism of BPVT is not well known, abnormal flow conditions in the new and native sinuses and lack of functional endothelialisation are suspected causes. BPVT may result in valve dysfunction, possibly related to degeneration, and recurrence of patient symptoms, or remain subclinical. BPVT is best diagnosed by multiphase gated CT angiography as the presence of reduced leaflet motion (RELM) and hypoattenuating aortic leaflet thickening (HALT). Whilst CT is used to exclude BPVT in symptomatic patients and those with increased valve gradient, the value of screening and prophylactic anticoagulation is debatable.

Abbreviations:

BPVT: bioprosthetic valve thrombosis
BPHV: bioprosthetic heart valves
TTE: transthoracic echocardiography
TOE: transoesophageal echocardiography
CT: computed tomography
RELM: reduced leaflet motion
HALT: hypoattenuating aortic leaflet thickening
SVD: structural valve degeneration

Introduction:

Severe aortic stenosis is prevalent in the aging population with an incidence of 4.4% per year in patients ≥ 65 years (1). Whilst surgical aortic valve replacement (SAVR) is the historical gold standard treatment in patients with symptomatic severe aortic stenosis, transcatheter aortic valve implantation (TAVI) initially provided a treatment option that is superior to medical therapy in inoperable and high-risk patients (2).
More recent randomised trials indicated non-inferior or better short-medium term clinical outcomes of TAVI versus SAVR in intermediate-risk patients (3) and low-risk patients (4). It is reported that each year, 180,000 patients could be considered potential TAVI candidates in the European Union and Northern-America, and this number might increase to 270,000 if the indications for TAVI were expanded to include low-risk patients (1). Whilst TAVI provides an alternative therapy to SAVR in inoperable and high-risk surgical patients with good short-medium term clinical outcomes, durable long-term outcome is important if the TAVI is to be offered to younger patients with lower surgical risk. Two key factors that may influence this is structural valve degeneration and leaflet thrombosis.

In this article we discuss the pathophysiology of bioprosthetic valve thrombosis (BPVT) and structural valve degeneration (SVD), their imaging findings, and the potential implications on clinical outcome.

**Bioprosthetic valve thrombosis**

BPVT is a recognised complication of surgical and transcatheter bioprosthetic heart valves (BPHV). The rate of BPVT varies significantly depending on the patient population, post-TAVI antithrombotic medication, diagnostic modality, and the definition of thrombosis. The incidence of BPVT is reported as 4% post-SAVR (5) and 13% post-TAVI (5). The incidence of clinically apparent BPVT thrombosis is much lower (0.6-2.8%) (6,7) (Fig 1 & 2), although significantly higher with valve-in-valve TAVI (7.6%) (8).

Reduced leaflet motion post-TAVI is more common in patients on dual antiplatelet therapy compared to those on warfarin (29% vs. 0%) (9). Thrombosis can occur within a few days after TAVI (10), although the reported median interval to BPVT in symptomatic patients is 181 days (interquartile range: 25-297 days) (7) and remains significant at one year (11). It has been proposed that lack of anticoagulation may contribute to valve dysfunction, which may affect valve longevity (12). Registry data from 2,555 patients revealed a 5.5% valve degeneration rate at 12 months, and anticoagulation was protective against valve degeneration (13). Whilst some studies have reported an association between subclinical leaflet thrombosis and transient ischaemic attack and stroke (5), others did not (14,15).
Mechanism of BPVT

The aetiology of TAVI thrombosis has not been fully elucidated, but likely to be multifactorial, with contribution from the components of Virchow’s triad (16). These are likely to be (i) device-related, (ii) rheological, (iii) haematological and (iv) patient-related factors.

(i) Device-related factors

Implantation of artificial surfaces such as a prosthetic valve that is primarily composed of collagen, which comes into contact with flowing blood results in contact activation of plasma coagulation. Proteins such as von Willebrand factor, fibrinogen, and fibronectin are adsorbed onto the artificial surface and bring about accumulation of components of the contact system on the valve (17), followed by adhesion of platelets and leucocytes, platelet activation and aggregation, and thrombin generation. This can eventually result in deposition of a platelet-rich thrombus held together by fibrin strands on the artificial valve surface. Endothelialisation of the bioprosthetic valve usually occurs around 3 months post-implant (18), but valve thrombosis continues to occur well beyond this time-window. The stented native valve itself may contribute to an ongoing thrombotic risk, since in patients with severe aortic stenosis, raised levels of tissue factor and activated factor XI have been documented, correlating with the degree of measurable thrombin generation in venous blood (19-21). The TAVI implantation procedure may also increase the risk of valve thrombosis. Crimping of the bioprosthetic valve leaflets into the delivery system, incomplete expansion, post-dilatation and incomplete apposition to the aortic wall have all been proposed as possible contributors to subsequent BPVT (22-24).

(iii) Rheological factors

Stagnant or static flow results in activation of coagulation, whilst turbulent flow can lead to platelet activation and neointimal trauma and disruption, and may increase the likelihood of local thrombus formation. Incomplete expansion or apposition of the prosthesis to the native aortic valve may produce complex localised flow patterns which promote fibrin deposition, platelet activation and thrombosis (22,25). High wall shear stress from the base of the valve leaflets toward the leaflet tips, where maximum flow activation occurs can promote platelet activation (26, 27). Prolonged
exposure of blood to these shear stresses (28-29) combined with flow recirculation may stimulate localised thrombogenesis (26).

The area between the prosthetic valve frame and the stented native valve leaflets is also recognised to be an area of low shear but with potential turbulent flow pattern which can create a prothrombotic milieu (6,27). It has also been proposed that supravalvular, rather than intra-annular, positioning of the prosthetic valve may reduce the risk of valve leaflet thrombosis (27).

(iv) Haematological factors

Regardless of the trigger (such as rheological factors or contact activation), the end result is activation of both platelet aggregation and the coagulation cascade. However, intrinsic defects in the coagulation pathways that promote a hypercoagulable state may also predispose to valve thrombosis. Procoagulant conditions such as inherited or acquired thrombophilias all increase the predisposition to thrombotic events (30). A testament to the crucial role of the coagulation pathway in valve leaflet thrombosis is that the thrombosis resolves with therapeutic anticoagulation and anticoagulation is also known to reduce restricted leaflet motion (31).

(v) Patient-related factors

The majority of TAVI recipients are elderly, often with multiple comorbidities that increase the risk of thrombosis after TAVI. Patient-related factors that increase the propensity for thrombosis include atrial fibrillation (AF), age, immobility, malignancy, smoking and renal failure (32), with AF being perhaps the most recognised risk factor. Most patients undergoing TAVI have a CHADS\textsubscript{2}VASC\textsubscript{2} score of at least 3 (usually 1-2 for age, usually accompanied by other vascular arterial disease or hypertension, which are extremely common in these patients). AF is frequently observed in this cohort, even when not previously reported (33), and underscores the need for a low index of suspicion for AF in this cohort, where new onset AF is reported in 14% post-TAVI (33).

Mechanisms of structural valve degeneration (SVD)

SVD is an acquired disease of the bioprosthetic valves and is defined as deterioration of the leaflets (eg. thickening, calcification, tearing) or supporting structures. These would adversely affect the valve hemodynamic and manifest in valular stenosis and/or
regurgitation (34). There is a continued interest to delve further into our understanding of the biology and mechanisms of SVD and BVF. In particular, this seems of importance in the context of the increasing focus on the treatment of valvular disease and increasingly in younger patients. From an imaging and radiological perspective, understanding of SVD mechanisms is imperative to guide the development of new imaging approaches to improve patient outcomes.

(i) Leaflet thrombus, fibrosis, and calcification

The patho-anatomical characteristics of SVD is determined from studies of explanted valves and the association of SVD with circulating biomarkers. On gross inspection, longer-term explanted valves frequently demonstrate leaflet tears, pannus or fibrosis, and/or calcification (Fig. 3; A&B), which lead to the restricted leaflet motion or insufficiency that can be observed on imaging the valve. The timing of leaflet thickening secondary to fibrosis and calcification in transcatheter explants was recently reported at greater than 60 days and greater than 4 years, respectively (Fig. 3; C&D) (35-36). However, an equivalent timeline of histological fibrosis and calcification across the many types of surgical bioprosthesis used since the 1960s is unclear. Notably, these timelines have the potential for bias given the 'snapshot in time' nature of explanted tissue. Long-term follow-up imaging studies have the potential for elucidating this in the future.

Studies in both surgical and transcatheter heart valves demonstrate that calcification can severely disrupt leaflet structure and function. Mineralisation is proposed to be the result of a combination of factors including biological response to matrix fixative materials (eg. glutaraldehyde), mechanical stress, and cellular infiltration (37-39). In fact, studies have demonstrated an association of surgical BPHV calcification and activation of pathways traditionally identified in vascular calcification, including expression of alkaline phosphatase and osteopontin (40-42). In addition to providing insights into fibrosis and calcification, studies of explanted transcatheter bioprosthetic valves reported histologically observable thrombus. However, rates varied considerably, which may be attributable to different histological methods and diagnostic criteria used in each study (35,36). Also reported was the predominate accumulation of thrombus at the base of leaflets on explanted transcatheter valves, as seen on computed tomography (CT) imaging. Yet establishing what is equivalent of leaflet thrombus histologically and the appearance of
hypoattenuating leaflet thickening (HALT) on imaging of either surgical or transcatheter heart valves remains to be seen (31,35,43). There is also still a need to establish if there is a direct molecular mechanism of leaflet thrombus as a driver of SVD. Importantly, future studies, such as the planned long-term durability analysis of the CT sub-study of PARTNER3 (44) will help to clarify any potential link between SVD and leaflet thrombus.

(ii) Cholesterol and inflammation

The presence of cholesterol in surgical bioprosthetic valves has been reported over many years in the explanted valves and patients with SVD have higher cholesterol levels (45-49). Oxidised low density lipoprotein (LDL) has also been found in degenerated BPHVs and is associated with inflammatory infiltrates. Moreover, blood levels of LDL and lipoprotein-associated phospholipase A2 have been found to be an independent predictor of SVD in SAVR patients (46,50,51).

While these studies propose a potential metabolic link to SVD, identifying specific risk factors or markers of SVD requires further study. Similarly, the debate on statin use to combat SVD remains, with conflicting results reported. Integration of molecular imaging techniques may allow for the evaluation of lipid and inflammatory infiltration to bioprosthetic valves akin to current atherosclerotic plaque approaches. Recently, Cartlidge et al. demonstrated that 18F-Fluoride uptake was associated with areas of SVD on histology on ex-vivo surgical BPHVs (52). However, further refinement of our understanding of the cellular and matrix processes being detected by 18F-Fluoride imaging is needed. The continued evolution of imaging and computing technologies also hold promise for understanding the pathophysiology of SVD. This includes applications of radiomics as well as computational fluid dynamics to understanding flow characteristics and shear stresses around the bioprosthetic valve to understand the causes of BPVT and degeneration.

Diagnosis of bioprosthetic valve thrombosis and degeneration

Valve thrombosis should be considered as a clinical and imaging spectrum, from subclinical, non-obstructive thrombosis to clinical-obstructive thrombosis (Fig. 1). The development of obstructive symptoms are dependent on the volume of thrombus, the number of leaflets involved, and the length of time from implant (9). Based on this
hypothetical concept, the echocardiographic signs of valve thrombosis are diverse, ranging from a totally normal appearance to complete valvular dysfunction.

Transthoracic echocardiography (TTE) is the primary imaging modality during follow-up for monitoring prosthetic valve function (Table 1; Fig. 4&5). European guidelines recommend baseline TTE evaluation within 30 days of implantation, at 1 year, and then annually afterwards. Earlier follow up studies should be considered when new symptoms occur (53). First-line screening of prosthetic valve dysfunction with TTE has limited value, as gradients could be normal despite valve thrombosis (32). BPVT should be considered when mean trans-prosthetic pressure gradient (mPG) is $\geq 20$mmHg, or when a $>50\%$ increase in mPG from baseline is observed (54-56) (Table 1). Leaflet thickening may be visualised (Fig. 4) as the echocardiographic correlate of HALT on CT (57). However, acoustic shadowing from the TAVI device may preclude adequate visualisation of the TAVI device leaflets (6) and transvalvular gradients depend on the type and size of the implanted valve, so unless there is a significant change from baseline gradients, TTE may not be sensitive enough to detect early haemodynamic changes in BPVT. Transoesophageal echocardiography (TOE) is reported to have comparable sensitivity to CT for the detection of leaflet thickening, thrombotic appositions, or restricted leaflet mobility (9), and though more invasive than TTE or CT, it could be considered when TTE images are suboptimal and in patients at increased risk of iodine-induced nephropathy. A deeper TOE longitudinal view with slight anterior flexion of the probe is recommended to avoid acoustic shadows created by the bioprosthesis scaffold.

ECG gated CT angiography is recognised as the gold standard imaging technique for the diagnosis of BPVT. CT diagnosis is based on the observation of reduced leaflet motion (RELM) and HALT on multiphase ECG gated CT angiography (9,12,58) (Fig 2 & 6). The leaflet thickening commences from the base of the leaflet and extends to the tip in more severe cases. Based on the extent of leaflet thickening (eg. basal vs. whole leaflet involvement), a semi-quantitative HALT grading system has been described (43). Leaflet thickening and/or calcification are observed in cases with leaflet degeneration (Fig. 7). Previous studies indicated that CT attenuation can be measured to differentiate pannus from thrombus ($\geq 145$HU and $<90$ HU, respectively) (59). It should be recognised that pannus and thrombus can coexist (60). When
Leaflets are not thickened or restricted, a prosthesis-patient mismatch should be considered as the cause of symptoms or abnormal transvalvular gradients (Fig. 7).

Leaflet motion and opening are evaluated on systolic phase images, and leaflet thickening may be observed in both systolic or diastolic images (Fig. 6). To reduce beam hardening artefacts from TAVI struts, CT is performed with a tube voltage of 120-140kV, the tube current is adjusted based on the patient’s body morphology. Beam hardening is less of an issue with stented and stentless SAVR and imaging at 100kV is feasible. Unless contraindicated, heart rate control strategies (e.g. beta-blockade and avoiding caffeine prior to the scan) should be considered to improve the visualisation of bioprosthetic valve leaflets.

Whilst retrospective ECG gating was recommended by previous studies (61), prospective gating with wide padding (e.g. 30-90%) may be considered to reduce radiation exposure. The imaging field can be limited to the TAVI structure and the left ventricular outflow tract (Fig. 8) to reduce radiation burden. Images are reconstructed with iterative reconstruction and thin slices (0.5-0.6mm) at 5-10% intervals. When available, ECG gated dual-energy imaging may be helpful to reduce beam hardening from the valve struts and improve visualisation of the leaflets.

**Management of bioprosthetic valve thrombosis**

There is no universal approach for the prevention of BPVT and/or routine imaging screening of BPVT (7). Routine anticoagulation is associated with increased bleeding risk, particularly in an elderly population, particularly intracranial haemorrhage (62). Current multisociety guidelines recommend administration of aspirin and 3 to 6 months of concomitant clopidogrel or vitamin K antagonist alone (63). Whilst the risk of BPVT is significantly lower with oral anticoagulation, the protective effectiveness of dual antiplatelet therapy is questionable (5,7). The routine application of non-vitamin K antagonist oral anticoagulant therapies for the prevention of BPVT had mixed results: one major trial (GALILEO trial) comparing the efficacy of rivaroxaban with antiplatelet regiments was prematurely terminated due to safety concerns related to increased all-cause death, thromboembolic events, and bleeding in the intervention arm (64). Another major trial (ATLANTIS) is ongoing (65). Preventive anticoagulation may be considered in patients at higher risk of BPVT (e.g. co-existing AF, valve-in-valve procedure) (7,66). BPVT is reported to
resolve in 88% of cases within 2 months of anticoagulation (6). The reported median
time to the reduction of transvalvular gradients is 14 days (7). In some patients, only
partial reduction in valve gradient and thrombus load may be seen due to the
organisation of the clot (7) and/or leaflet fibrosis.

The routine application of follow-up CT imaging at specified intervals is not currently
recommended (43). CT or TOE should be considered in patients with recurrent
symptoms (exertional dyspnea and stroke), increased gradients or new transvalvular
regurgitation.

**Conclusion:**

Bioprosthetic valve thrombosis is a complication of the TAVI procedure. BPVT may
result in the recurrence of symptoms in only a subset of patients, depending on
thrombus load. The emerging evidence indicates that thrombosis may lead to valve
degeneration. Imaging investigations play a fundamental role in the diagnosis of
BPVT and should be considered in suspected cases. Increased awareness of this
potential complication, including its potential impact on longer term valve function
and stroke risk, together with future development of imaging and haematological
biomarkers may help earlier identification of high risk patients and those with
subclinical BPVT that would benefit from anticoagulation.
References:


47. Farivar RS, Cohn LH. Hypercholesterolemia is a risk factor for bioprosthetic valve calcification and explantation. The Journal of thoracic and cardiovascular surgery 2003;126:969-75.


Table legends:

Table 1: Echocardiographic (TTE/TOE) signs of aortic bioprosthetic valve thrombosis.

Figure legends:

Fig. 1. The clinical and imaging spectrum of bioprosthetic valve thrombosis (BPVT).

In the early stages of BPVT, the patients may not be symptomatic or have significant transvalvular gradients on echocardiography. An increase in leaflet thrombus load and/or leaflet fibrosis results in valve restriction, increased transvalvular gradients, and recurrence of symptoms. Physicians should be aware that the symptoms and gradient changes may initially be mild, and early identification would aid appropriate earlier management.

Fig 2. Sub-clinical TAVI thrombosis.

81 years old patient referred for a CT scan to investigate the cause of hoarse voice and weight loss, 45 days post TAVI. Ungated contrast-enhanced CT demonstrated no cause for the presenting symptoms. The incidental finding was hypoattenuating leaflet thickening indicating thrombosis (HALT; A&B). Transthoracic echocardiogram (performed prior to CT) demonstrated a mean trans-prosthetic gradient of 10mmHg that reduced to 2mmHg following anticoagulation. The patient was treated with non-vitamin K antagonist oral anticoagulant. A follow up CT demonstrated resolution of the thrombi, 4 months following treatment (C&D).

Fig 3. Examples of features of bioprosthetic aortic valve pathology seen on gross examination at explant and on histology. A&B: surgical BPHV explants demonstrating grossly observable fibrosis and calcification on the aortic aspect of pericardial leaflets. C. Leaflet thickening as the result of fibrosis on an explanted
transcatheter aortic valve leaflet seen on histological cross-section staining with Movat’s Pentachrome stain. D. Severe calcification of an explanted aortic transcatheter BPHV pericardial leaflet shown on histological section stained with Movat’s pentachrome.

Fig 4. Bioprosthetic leaflet thickening on echocardiogram and CT in a patient with transcatheter aortic valve thrombosis.

Modified trans-oesophageal long axis echocardiographic view of the bioprosthetic aortic valve shows wedge-shaped thickening of the valve leaflet (yellow arrow) with correlating CT image (red arrow; B). Follow up imaging 3 months after anticoagulation therapy documents resolution of basal leaflet thickening (C).

Fig 5. Colour paucity sign on echocardiogram in a patient with bioprosthetic valve thrombosis.

80-year-old man presented with transient ischaemic attack 2 months after TAVI. Transoesophageal echocardiogram showed leaflet thickening (arrow, A) and the “colour paucity” sign, a filling defect in colour flow caused by the thrombus (black arrows, B). A peak trans-prosthetic velocity of >4m/s indicates severe stenosis (C). 3D echo images (D) demonstrated thrombi on valve leaflets (open arrow).

Fig 6. Bioprosthetic aortic valve thrombosis on CT.

82 years old patient presenting with high trans-prosthetic gradients on echocardiogram, 4 months after transcatheter aortic valve implantation (27mm Lotus, Boston Scientific). The leaflets were not visible on transthoracic echocardiogram (TTE). CT demonstrated moderate hypoattenuating leaflet thickening (HALT) extending to the leaflet tips (A). Mid systolic images (B) demonstrated reduced leaflet
Follow up CT 6 months after oral anticoagulation showed partial resolution of the HALT (C) and improved valve opening (D). Follow up TTE confirmed reduction of the mean trans-prosthetic gradient from 28mmHg to 10mmHg.

Fig 7. The spectrum of valve disease in patients with increased trans-prosthetic gradients.

Valve thrombosis demonstrated on axial and coronal multiplanar CT reformats (A: reduced leaflet motion; B: Hypoattenuating leaflet thickening). Degenerated transcatheter bioprosthetic leaflet calcification is seen in a patient with previous transcatheter aortic valve implantation within a calcified homograft (C & D). Image D & E shows an under-deployed transcatheter aortic valve (34mm Medtronic Evolut R; Minneapolis, MN) as a result of heavy native valve calcification with resultant small valve area for patient's size. The mean trans-prosthetic gradient was 32mmHg following implantation of the valve (E&F).

Fig 8. CT imaging of bioprosthesis.

Scout image (A) is used to identify the bioprosthesis (arrow) and plan limited field of view (yellow box) CT angiogram (8cm coverage in z axis). The resultant dose length product (DLP) was 175 mG.cm.